

Ion Transport of Two-Dimensional Materials

Subjects: Others

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Ion transport is one of the basic principles of the development of various different technologies that can improve the quality of our lives, such as the ever-growing importance of clean and sustainable energy, the reduction of water scarcity and even the improvement of fundamental medical application knowledge. Ion transport can be defined as the movement of charged ions from one position to another in ion electrolyte solutions within both organic (living cells) and inorganic (polymer materials) systems. Ion transport can be encouraged through various mechanisms such as electrochemical diffusion, ion active transport requiring external energy or bulk transport for the conversion of adenosine triphosphate (ATP) and energy consumption in biological functions.

Keywords: ion transport ; capacitance ; 2D materials ; multifunctional energy storages ; stimulus-responsive microsupercapacitor ; fluorescence imaging ; molecular transport

1. Introduction

Ion transport is one of the basic principles of the development of various different technologies that can improve the quality of our lives, such as the ever-growing importance of clean and sustainable energy, the reduction of water scarcity and even the improvement of fundamental medical application knowledge. Ion transport can be defined as the movement of charged ions from one position to another in ion electrolyte solutions within both organic (living cells) and inorganic (polymer materials) systems. Ion transport can be encouraged through various mechanisms such as electrochemical diffusion, ion active transport requiring external energy or bulk transport for the conversion of adenosine triphosphate (ATP) and energy consumption in biological functions ^[1]. This can be clearly seen in the sodium/potassium (Na^+/K^+) ions exchange pump, which is an important ion transportation mechanism that generally occurs in living cell membranes such as plant and animal cells ^{[1][2]}. For example, the electric eel possesses a system which demonstrates the evolution of biological membranes under ionic concentration gradients that provide ion transport for power generation. By combining a number of membranes with highly packed selectively ionic channels, electric eels can produce a strong current density which can discharge up to 600 Volts ^[3]. Ion transportation can be used as a potential way of understanding the mechanism involved in order to explore the mimicking effect of artificial membranes for various ion transport-based applications such as film-based catalysts for gas production (hydrogen and oxygen evolution reactions) ^{[4][5]}, energy storages (capacitors and batteries) ^{[6][7][8]}, and membranes for ionic and molecular separation ^{[9][10][11]}. Instead of artificial membranes in living cells, ions transport can also relate to cell stabilities, helping us to understand the fundamental mechanisms of ion transport in vitro and in vivo ^[12].

Two-dimensional (2D) materials are emerging categories of nanostructure materials which include graphene ^{[13][14]}, transition metal dichalcogenides (TMDs) ^[15], hexagonal boron nitride (h-BN) ^[16], and MXene ^[17]. The structure of these 2D materials can be controlled in many forms, including being stabilized in single or multiple layers or forming heterostructures, offering unique properties (electrical, thermal, optical and electrochemical, to name just a few) when compared to higher dimensional materials in bulk form ^[18]. For example, graphene displays higher levels of conductivity (including electrical and thermal conductivity) and a higher surface area than graphite ^[19]. Meanwhile, TMDs provide better optical properties than graphene materials due to their tuneable band gaps, which can be modified by reducing material thickness and used for optical applications in the visible spectrum. In addition, h-BN is categorized as an insulator that has a smooth surface and only a minimal lattice mismatch with graphite ^{[20][21]}. This leads to ultrahigh carrier mobility in graphene when it is integrated with h-BN ^{[22][23]}.

The review describes the fundamental properties of capacitance and ion transport in various 2D materials, and offers novel applications based on various potential technologies from the macro to the nanoscopic perspective. The review describes a well-known capacitance models, including the Helmholtz, Gouy-Chapmann and Stern-Otto models, as well as the capacitive model in two dimensional materials, which explain their ion transport properties. We also show that, in addition to energy storages (i.e., supercapacitors and osmotic energy), the ion-transport devices (i.e., the stimulus-responsive microsupercapacitors) can generate new functionalities through their response to the external stimulus. Such

functionalities include direct visualization of energy storages, light-induced energy storage and photodetections, and ion transport controls, as shown in **Figure 1**. These prominent, man-made technologies imitate the ion transport in living cells. To understand the extended capabilities of ion transport in artificial devices, it is important to connect with natural phenomena in living bacterial cells. This review aims to provide a better understanding of fundamental knowledge of ion transport technologies in order to examine further potential applications.

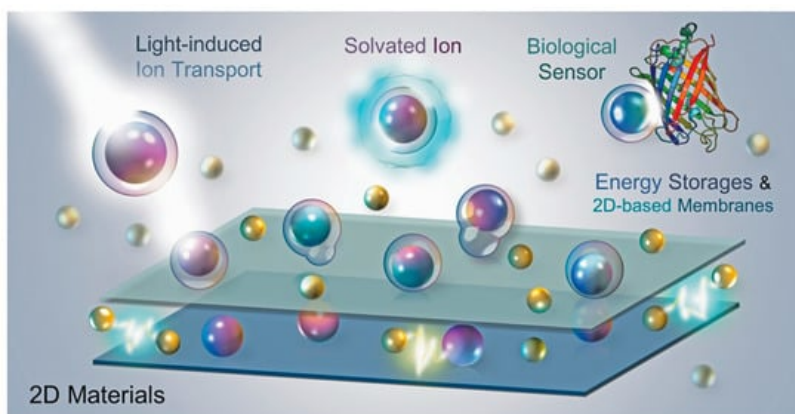


Figure 1. Diagram showing the potential applications of ion transport through two-dimensional (2D) materials, including the energy storages, 2D-based membranes for water purifications and energy harvesting (blue energy), light-induced ion transport, and biological sensors.

2. Principle of Ion Transport

The cations and anions can be separated out due to the charged channel surface. This is because the opposite charged ions (the counter-ions) would preferentially transport through the surface-charged channel faster than the same charged ions (co-ions). This is so-called ion selectivity which is based on the electrical double layer (EDL) structure of the charge distribution at the interface between a charged electrode surface and the surrounding electrolyte solution. The phenomena occurs via electrostatic interaction at which the charged channel surface attracts the counter-ions and repels the co-ions (**Figure 2 a**) [1][24], This results in a decrease in co-ions concentration and an increase in counter-ion concentration. This causes the local potential to decrease as a function of the charged electrode surface-electrolyte distance, as shown in **Figure 2 b**. The two layers are the stern layer and the diffusion layer. The stern layer, known as the compact (rigid) layer, possesses two planes. The first plane, which is located at the surface, contains solvent molecules and charged ions adsorbed tightly onto the charged surface. The adsorbed ions are defined as specifically adsorbed ions (counter-ions) at which point they are not solvated. Moving further away into the second plane, solvated ions are then encountered due to their increase in solvated ions size which is unable to reach near the surface. The interaction between the solvated ions and the charged surface is governed by coulombic forces as the solvated ions are non-specifically adsorbed [24][25][26]. The diffuse layer lies beyond the stern layer, in which the solvated ions start to be more scattered and increasingly less ordered when stepping away from the charged surface. The ion distribution of this layer is influenced by coulombic interactions between charged ions and charged electrode surface, and thermal motions. This indicates that the potential-distance profile has two regions that are linear (stern layer) and non-linear (diffuse layer), where the potential decay as a function of distance from the charged electrode surface (**Figure 2 b**). The density of solvated ions in the diffuse layer is much tighter at high electrode potential and less tight when they are away from the charged surface [24][25][26]. This causes the exponential decrease in potential as a function of diffuse layer distance. Moreover, the thickness of the EDL also relates to the Debye screening length (λ), which depends on the ionic strength (I) of the electrolyte, corresponding to $\lambda \propto I^{-1/2}$ [27]. For the nanocapillary channel, the thickness of the EDL plays a crucial role in ion transport, at which the EDL of the opposite charged surfaces are overlapped together. This can be attributed to the formation of almost a unipolar ions in the channel (abundant counter-ions), which can be observed in ion selectivity during transport through the channel, as shown in **Figure 2 c**.

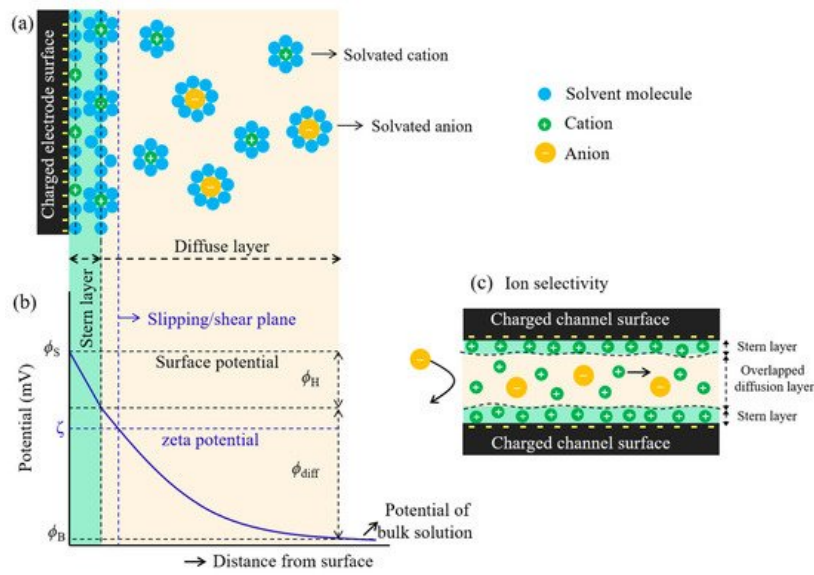


Figure 2. Schematic illustration of the electrical double layer (EDL). (a) The model of the EDL of the charged electrode surface immersed in the electrolyte solution at which negative potential bias is applied. (b) The potential profile of the electrode surface to the solution, which consists of the two steps of the decreasing potential as a function of the electrode distance. ϕ_s , ζ , and ϕ_B represent the potential at the electrode surface, slipping/shear plane (zeta potential), and the bulk electrolyte solution, respectively. ϕ_H and ϕ_{diff} are the potential of the Helmholtz plane and diffuse layer, respectively. (c) Ion selectivity inside the charged channel shows the two EDLs between the charged surfaces (overlapping diffuse layers), which allows counter-ions to pass through the channel but excludes co-ions.

The process of ion transport in nanochannels has received a great deal of attention. This plays a crucial role in the development of nanofluidics, ion sieving [9][11][28], and other nanoscale technologies such as energy storage [4][29], active ion gated control [30], and ion rectifications [31]. This has inspired various research directions into the fabrication of synthetic nanochannels from inorganic materials with well-defined properties (various types of geometries) and studying the mechanisms of ion transport [32]. As a development in nanochannel fabrication, this can allow researchers to study electrokinetic models of the transport of electrolyte ions through nanometer-sized slits [33][34][35]. Nanochannels can initially be fabricated from silica (lab-on-a-chip) with a height of 100 nm (Figure 3 a) [35], and it was found that a steady conductance at low salt concentrations inside the nanochannels results from the dominance of surface charge density in the nanochannels. This leads to the effectiveness of the surface charge density in the nanochannels, leading to the abundance of counter-ions which results in electroneutrality inside the channels [34][35]. Schoch et al. [34] increased the surface-area-to-volume-ratio by reducing the height of channel to 50 nm (Figure 3 b), showing that the surface charge plays a crucial role as a greater fraction of the total charge is attached to the channel's wall. This is attributed to the regulation of ionic flow inside the charged nanochannels.

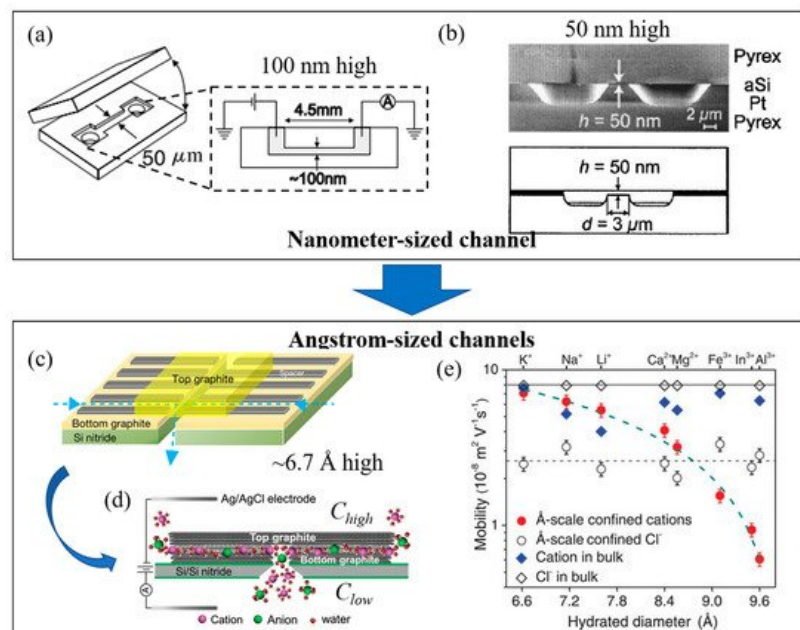


Figure 3. Schematic illustration of the fabrication of slits in nanometer-sized channel (top image) and angstrom-sized channels (bottom image). (a) Nanochannel assembly with cross-sectional side view (100 nm high). (b) Cross section of

nanochannels (50 nm high) as defined by the thickness of the silicon layer and the nanochannel length ($d = 3 \mu\text{m}$). (c) Schematic of graphene capillary devices showing the composition of each device. The arrow indicates the flow direction of electrolyte. (d) Schematic of ion transport under nanocapillary channels (channel height = $\sim 6.6\text{--}6.7 \text{ \AA}$) driven by the drift-diffusion techniques. (d) The individual ion mobility in \AA -confined channels (using bilayers of graphene as spacers between the materials) as a function of hydrated diameter, which were compared to their ion mobilities in bulk solutions. Reprinted with permission from (a) ref. [35] Copyright (2004) American Physical Society (United States), (b) ref. [34] Copyright (2005) American Institute of Physics (United States), (c) ref. [36] Copyright (2016) Macmillan Publishers Ltd., and (d,e) ref. [37] Copyright (2017) The American Association for the Advancement of Science.

To control ionic current during the transport of ions through a channel, the height of the channel should be less than the Debye screen length (1–100 nm in height) and the channel's wall should be charged [38]. A unipolar solution of counterions can be created inside the nanochannel at the electrolyte concentration neutralizing the surface charge, while the coions are electrostatically repelled from the channel's wall. This creates the ionic current inside the channel which depends on the surface charge density in the concentration – although the ionic current becomes less involved in surface charge density where the bulk concentration increases [31][38]. The height of the channel should be similar to the nanoscale channels inside transmembrane proteins, which control the transport of ions and molecules. As the magnitude of the EDL is evaluated from the Debye screening length, which relates to the ionic concentration, this causes the overlapping EDL inside the channel depending on the relation between size of channels and the ion concentration. Due to traditional synthetic channels with heights in the range of 1–100 nm, the EDL overlap can occur at very low concentrations ($<10 \text{ mM}$), which is far lower than the concentrations observed in physiological solutions [30]. Duan et al. [30] demonstrated ion transport by reducing the size of nanochannel to 2 nm in height, providing the connecting EDLs from each side of channel's wall at 100 mM concentration, which is close to physiological concentrations. The fluid nanochannels thus obtained can be used to mimic protein channels in order to study the ion/molecular transport in liquid nanoconfinement [30][31][32].

Although an SiO_2/Si -based nanochannel with a 2 nm height with hydrophilic surfaces showed almost four-fold increase in ion transport when compared to a 25 nm height channel in terms of bulk ion transport, but the mechanism behind the process is not fully understood [30]. The process may result from the overlapping of the hydrogen bonding network of the two hydration shells next to the hydrophilic surfaces [30]. To understand and prove this, the hydrophobic nanochannels should be fabricated under the same experiment conditions. Jung et al. [39] first fabricated rectangular-shaped nanochannels using graphene nanosheets across the surface to provide the hydrophobic nanoconfinement [39][40]. They found that the 3.6 nm graphene-based nanochannels performed an excellent level of ion transport, providing great ionic conductance by over two orders of magnitude compared to the nanochannels in the absence of graphene coating in an aqueous solution. This can be explained by the fact that the surface of the graphene nanochannels is much cleaner and smoother than that the SiO_2/Si nanochannels (10–50 nm height channels showing significantly low ion transport).

3. Ionic Sieving through 2D Material-Based Membranes

A membrane can be defined as a thin physical interfacial material which possesses specific chemical and/or physical properties to control a selective species (i.e., charged ions/molecules, live cells, and various size of particles) passing through. In general, it can be classified by cross-sectional properties into isotropic membranes (homogeneous composition; microporous, nonporous dense, and electrically charged membranes) and anisotropic membrane (heterogeneous composition; Loeb-Sourirajan and thin-film composite membranes) [41][42]. As the various structures and function inside membranes, this can be used to control the transport of permeants which is based on pore size of membranes, diffusion (driven by concentration or pressure), and electrostatic repulsion. The different types of membranes are widely implemented for various filtration technologies such as particle separations (large molecules, gas, and ions), pervaporation, and reverse osmosis (RO) membranes. Electrically charged membranes can be classified as positively or negatively charge functional groups in the structural materials, which is so-called an anion-exchange membrane (AEM) and a cation-exchange membrane (CEM), respectively [41]. The mechanism of separation is mainly based on the electrostatic repulsion of the similar charge between the charge inside the membrane and charge of particles under the influence of an applied electric potential. The ion-exchange membranes (IEM) can be produced from various materials such as organic (e.g., liquid and polymer) [43][44], inorganic (e.g., carbon nanotube, graphene, transition metal dichalcogenides) [9][11][45], and organic-inorganic hybrid (e.g., metal organic framework) materials [46][47][48].

Membrane potential is defined as the electrical potential arising from the difference in ionic concentrations on each side of a semipermeable membrane. It is also known as transmembrane potential, and the phenomenon has been widely studied in biological cell membranes such as neurons and muscle cells. The application of an electric field across the membrane

allows us to determine the charge and size selective ion sieving through the nanoporous graphene (NPG) membranes [49], angstrom-scale slits [37] and laminar stacked 2D membranes [9][10][11][50]. The principle of membrane potential will be discussed in this section in the context of the model used.

The Nernst equation is used to determine the equilibrium state of the membrane when the membrane is permeable to only a single type of ion. However, if several types of ions on both sides are involved in the flow through the membrane (i.e., the membrane is permeable to various ions) then membrane potential can be evaluated using the Goldman-Hodgkin-Katz (GHK) equation, which allows the selective determination of ion. This equation is an extended version of the Nernst equation.

Based on the assumption of the GHK equation [51][52], the electrodiffusion model is used to assume the flow of an ion through the membrane, which is associated with various conditions. The conditions considered are based on a homogeneous slab of material (one that is uniform, planar and infinite in its lateral extent), a constant electric field (the potential decreases linearly within the membrane), a material in which ions can move across the membrane independently (without interacting with one another), and have constant permeability, P , (where $P = \beta D / l$; β , D , and l are the partition coefficient, the diffusion coefficient, and the membrane thickness, respectively) [1][52][53][54]. In this assumption, the x -axis is used to represent the direction of the flow of ions through the membrane. Thus, the origin of the flow lies at the interface of the membrane on the feed side (denoted $x = 0$) and its termination is the interface of the membrane at the permeate side (denoted $x = l$) when the membrane thickness is l , as shown in **Figure 4 b**. As the membrane is assumed to have lateral uniformity, variations in the electric field (E_m) and ionic concentration (C_i) within the membrane are related only to the x -direction. The assumption under the GHK model is that the field inside the membrane is constant and equal to: $(12) dE/dx = E_p - E_f / l = -E_m / l$ where E_m is the transmembrane voltage, E_p and E_f are the potential at the permeate and feed sides of the membrane surface, respectively.

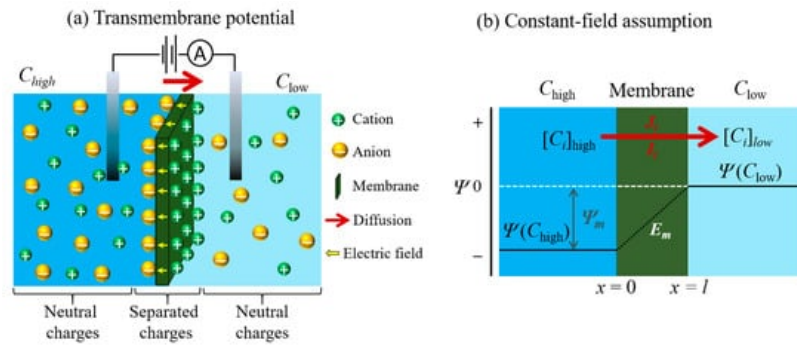


Figure 4. (a) Schematic of ion transport through a semipermeable membrane (a cation-exchange membrane in this example) showing the difference in ion concentration between two liquid reservoirs separated by the membrane. The red and yellow arrows represent the diffusion force and migration direction within the membrane, respectively. (b) Electrodifffusion model in the membrane illustrating the constant field assumption. According to Goldman's Assumption, the electrical field is the same at all positions along the membrane thickness ($dE/dx = \text{constant}$). The field is the electric potential difference between two liquid reservoirs ($E_{\text{permeate}} - E_{\text{feed}}$) through the membrane thickness (l). The flow of ions (i) across a semipermeable membrane is related to a molar flux (J_i) and electric current density (I_i). The ionic concentration and the electric potential in the membrane are C_i and E_m respectively. Note the reduced potential (Ψ) is $\Psi = FE_m/RT$.

4. Optical Induction with Ion Transport and Optical Techniques for Ion Transport

The utilization of optical techniques for ion transport have recently become available through optical induction [55] and optical investigation [12], but fundamental mechanisms are more ambiguous. It is important to investigate these methods and the extension of boundaries further in biological simulation and manmade applications.

To enhance the effects of ion transport, the structural designs of 2D materials can be used to reengineer the ways in which ions propagate, with a significant jump in the super-diffusive regime [56][57]. When restricted by a 2D planar surface, the diffusion in normal and anomalous diffusion (the sub-diffusive and super-diffusive processes) is a quintessential property. Since our understanding of ion diffusion is a foundation of ion transport, few articles have studied the subject via simulation [56] or experiments [58].

Although photoelectric stimuli occur for ion transport induction, responses from photothermal effects have also been investigated [59]. In stacking MXene nanochannels, the reduction of temperature of Gibbs free energy on light irradiated regions causes non-isothermal ion transport, shown in **Figure 5 d**, with a response of up to 1 mV per degree Kelvin. This

also sheds light on photothermal ionic transport applications, which have the potential for 1.68 mWm⁻² output [59].

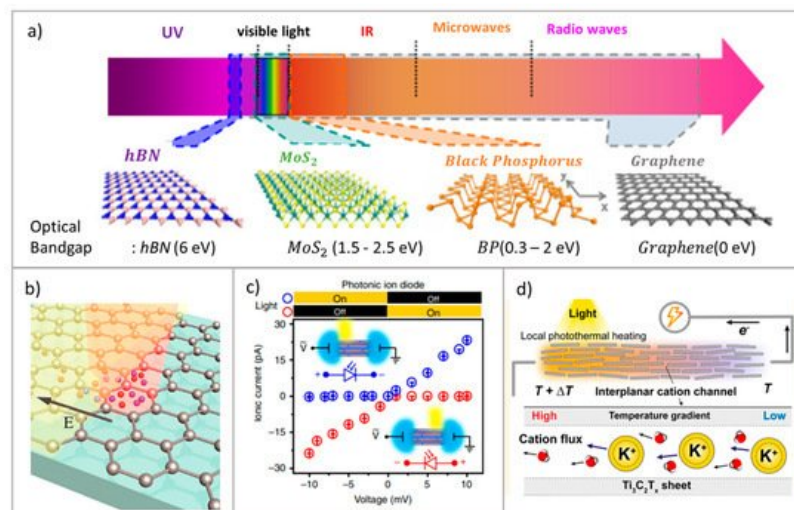


Figure 5. (a) 2D materials and optical bandgaps [60]. (b) Photo–Dember effect for increasing a local charge density [61]. (c) Photogate effect induces a directional ion transport via nanoscopic channels [62]. (d) Temperature gradient induces ion transport due to local charge density gradient [59]. Reproduced with permission from (a) ref. [60] Copyright (2014), Springer Nature; (b) ref. [61] Copyright (2014), American Chemical Society; (c) ref. [62] Copyright (2019), Springer Nature; (d) ref. [59] Copyright (2020), American Chemical Society.

Fluorescent markers can be utilized for ion transport in neuron cells, and can also be used to indicate molecular interactions and transport through bacterial membrane [63][64][65]. With more complicated pathways because of their molecular specificity, the transport of ions or charged molecules relates to mechanisms of ion transport through nanopore (1D diffusion) and on membrane surfaces (2D diffusion) [66]. The transport of charged molecules in respect of ion transport utilizes fluorescent techniques for fundamental investigation [67]. Charged molecules of antimicrobial peptide (AMPs) were reported to have been transported through the bacterial membrane [63].

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