Analytical Methods for Detection and Quantification of Neurotransmitters

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Recognized for its speed and selectivity, high-precision liquid chromatography with an electrochemical detector (HPLC-ECD) enables direct analysis of intracerebral microdialysis samples without complex derivatization. Various chromatographic methods, including reverse phase (RP), are explored for neurotransmitters (NTs) and metabolites separation.



1. Introduction

Monoamine neurotransmitters (NTs) are a class of NTs that include brain chemicals involved in the transmission of signals between nerve cells, or neurons. The two main types of monoamine NTs are catecholamines and indolamines: catecholamines include dopamine (DA), norepinephrine (NE), and epinephrine (E) and indolamines include serotonin (5-hydroxytryptamine or 5-HT).

These monoamine NTs play a crucial role in the regulation of various physiological and behavioral processes, such as the regulation of mood, sleep, appetite, reward, attention, and stress. Imbalances in the functioning of monoamine NTs are associated with various neurological and psychiatric disorders.

2. Analytical Methods for Detection and Quantification of NTs and Metabolites

The analysis methods have been developed for the detection and quantification of NTs in vivo to understand specific neurotransmission dysfunctions in neurodegenerative diseases or in psychiatric disorders.

2.1. Gas Chromatography and Capillary Electrophoresis

Gas chromatography (GC) ^{[1][2]} and capillary electrophoresis (CE) ^{[3][4]} are analytical techniques used in these research areas. However, they have several drawbacks: GC requires the use of compound derivatization to make them more volatile ^[5], and CE is a limited technique for the analysis of complex mixtures. HPLC, on the other hand,

allows for the analysis of biological samples from microdialysis without the need for chemical derivatization or extraction steps.

2.2. HPLC

Since the late 1980s, research teams led by Donzanti et al. ^[6], Peinado et al. ^[7], and Rogers et al. ^[8] have focused their studies on the detection of amino acid neurotransmitters, particularly γ -aminobutyric acid (GABA), achieving a sensitivity of about 0.1 nM. HPLC analysis of NTs is characterized by its speed and selectivity. Typically, a reverse-phase (RP) system is used to separate NTs due to their hydrophobic nature. For instance, Bidel et al. developed an HPLC method for the separation of monoamines and their metabolites. They achieved a total elution time of about 12 min, a minimum resolution between each peak of 2.2, and a number of theoretical plates (N) ranging from 2900 to 3800 ^[9]. These values are largely sufficient to validate the use of HPLC.

By way of comparison, Reinhoud et al. developed a UHPLC method similar conditions under reverse phase conditions, enabling the separation of NTs in a 12 min run time elution. The columns of UHPLC have smaller particle sizes. Consequently, chromatographic peaks will be finer and better defined, allowing for improved separation of compounds. Moreover, the number of theoretical plates in this study has been estimated to be close to 200,000 ^[10].

More recently, hydrophilic interaction liquid chromatography (HILIC) columns have been employed ^{[11][12]}. These columns offer reduced system pressure, allowing for enhanced flow rates and shorter analysis times. For example, in the study by Zhou et al., the use of a low-granularity column (1.7 μ m) combined with a flow rate of 0.4 mL min⁻¹ is employed. These experimental conditions result in very short analysis times, on the order of 4 min. It is noteworthy that the Multiple Reaction Monitoring (MRM) mode of the mass spectrometer enhances the selectivity of the measurements ^[13].

The utilization of HILIC column necessitates coupling with mass spectrometry because of its incompatibility with the salts used with the electrochemical detection.

2.3. Detection of NTs and Their Metabolites

Various types of detectors can be employed, including fluorescence detectors (FLD) ^{[14][15][16]}, mass spectrometry (MS) ^{[17][18][19]}, sensors and biosensors ^{[20][21][22]} or electrochemical detector (ECD). ECD holds an advantage over MS detectors due to its lower operating cost and easy maintenance. For instance, weekly polishing of a glassy carbon (GC) working electrode with alumina powder is adequate to maintaining a reflective surface, thereby enhancing result repeatability and reproducibility.

ECD has also been extensively utilized for the detection and quantification of NTs and their metabolites ^{[23][24][25]} ^[26]. It proves to be a straightforward and sensitive method for quantifying small amounts of NTs. One of its notable benefits is its simplicity and minimal maintenance. Several types of electrochemical detectors exist, including coulometric and amperometric detectors. The principle of the coulometric detector lies in the measurement of the current charge produced during electrolysis at a constant potential. Compounds are then oxidized or reduced almost entirely. Coulometric detectors are less sensitive to variations in flow rate and temperature than amperometric detectors. However, electrodes are easily contaminated due to their large electrolysis surface area. The measurement of the charge during the electrochemical reaction is based on Faraday's law (Equation (1)).

 $Q=n F N_O$ (1)

with Q the charge (C or A s), n the number of electrons exchanges during the electrochemical detection, F the Faraday's constant (96,485 C mol⁻¹) and N_0 the number of moles of the O compound.

Amperometric detection generally provides high sensitivity and the response remains linear over a wide range of concentrations. For these reasons, they are more widespread than coulometric detectors. Compared to coulometric detection, electrolysis consumes only about 10% of the analyte. The value of the measured current in an amperometric detector depends on the geometry of the electrode used (**Table 1**).

 Table 1. Limiting current equation as a function of geometry electrode used during the amperometric detection [27].

Electrode Geometry	Limiting Current Equation
Tubular	i=1.61nFC _O (DA/r) ^{2/3} v ^{1/3}
Planar, parallel flow in channel	i=1.47nFC _O (DA/b) ^{2/3} v ^{1/3}
Planar, perpendicular flow	i=0.903nFC ₀ D ^{2/3} v ^{-1/6} A ^{3/4} U ^{1/2}
Wall jet	i=0.898nFC ₀ D ^{2/3} v ^{-5/12} a ^{-1/2} A ^{3/8} v ^{3/4}

With: i the intensity (A), C_O concentration of the O compound (mol cm⁻³), D the diffusion coefficient (cm² s⁻¹), A the elegtrates of the diffusion coefficient (cm² s⁻¹), A the elegtrates of the diffusion coefficient (cm² s⁻¹), A the elegtrates of the diffusion coefficient (cm² s⁻¹), A the elegtrates of the diffusion coefficient (cm² s⁻¹), A the elegtrates of the diffusion coefficient (cm² s⁻¹), A the elegtrates of the diffusion coefficient (cm² s⁻¹), A the elegtrates of the diffusion coefficient (cm² s⁻¹), A the elegtrates of the diffusion coefficient (cm² s⁻¹), A the elegtrates of the diffusion coefficient (cm²) and the diffusi

For electroactive compounds, charge can be correlated with the moles of the considered compound, extending to concentration. It is crucial to emphasize that the number of electrons exchanged in the electrochemical reaction is contingent on the applied potential. If the overvoltage is insufficient, then the electrochemical reaction remains incomplete.

ECD has some limitations: this detector is not universal and compounds must be electroactive to be detectable. In the same domain, GABA, a neurotransmitter involved in neurodegenerative diseases ^{[28][29]}, can be analyzed by HPLC-ECD. However, GABA is not electroactive and requires chemical derivatization. In the Panrod et al. study, two derivatization pathway involving aldehydes moieties have been employed to be able to detect GABA ^[30].

Therefore, the development of a single analytical method for all NTs with an electrochemical detector appears to be challenging in light of the mentioned limitations.

The two most frequently employed working electrode materials are GC and boron-doped diamond (BDD). These materials showcase diverse physicochemical characteristics: the BDD electrode boasts the largest electrochemical window, facilitating the detection of numerous electroactive compounds. However, as indicated in the study by Zhang et al. in 2016, a high overpotential seems to reduce the peak area of the analytes. The sensitivity of electrode passivation is higher for a BDD electrode compared to a GC electrode ^[31]. Consequently, it seems that reproducibility is superior with a GC electrode.

The GC electrode exhibits a narrower electrochemical window compared to the BDD electrode. Consequently, the analysis range is restricted, and the oxidation of water impedes the detection of compounds with high oxidation potentials ^[32]. Analyzing compounds with potentials involving reduction is impossible due to the reduction of dissolved oxygen ^[33]. Ultimately, the choice between the two electrodes depends on the application when the compounds have relatively low oxidation potentials. Then, it is preferable to use a GC working electrode.

To enhance the sensitivity of NTs detection, two optimizations are considered: firstly, increasing the surface-tovolume ratio of the electrochemical cell, and secondly, using a modified electrode material to enhance its physicochemical characteristics. In the study by Xu et al., the working electrode on GC is modified through an electrochemical reaction with poly(para-aminobenzoic acid) (P-pABA) ^[34]. With a 0.7 V vs. Ag/AgCl potential detection, the sensitivity of measurement improved from 8.5 nA to 23 nA, 11 nA to 23 nA, 7 nA to 16 nA, 9 nA to 25 nA and 4 nA to 23 nA for 5-HIAA, 5-HT, DA, DOPAC and HVA, respectively. Augmenting sensitivity enhances the quantification of NTs.

In conclusion, the ECD is widely employed for the detection of monoamines due to its user-friendly nature and low maintenance cost. Its sensitivity enables the quantification of very low concentrations of NTs. To expand the capabilities of this detector, it would be possible to develop chemical derivatizations either directly on the compounds or on the electrode surface. These chemical modifications could induce a broader spectrum of applications.

2.4. Limit of Detection and Quantification

By convention, the limit of detection (LOD) and limit of quantification (LOQ) are established at signal-to-noise ratios of 3 and 10, respectively. The linear range (L.R.) denotes the measurement zone where the device-recorded signal is directly proportional to the quantity or concentration of the substance being measured.

Table 2 compiles the various values of LOD, LOQ, and the linear range for the NTs and their metabolites. Additionally, the different experimental conditions have been reported for informational purposes. The studies are ranked based on the particle size of the chromatographic C_{18} column used, from smallest to largest. The list of presented publications is not exhaustive. Other articles have been published on the use of HPLC-ECD but they did not detail the analytical development and LOD/LOQ of NTs. Those articles were not included in this summary table.

For instance, one can cite several recent works by Guo et al. (2023) [35], Lei et al. (2023) [36], and Wang et al. (2022) [37].

According to these studies, the sensitivity of the targeted molecules can approach values close to 10^{-9} mol L⁻¹ for HPLC system and less, close to 10^{-11} mol L⁻¹, in UHPLC cases. As mentioned earlier, the use of columns with small particle sizes refines elution peaks and consequently lowers quantification limits. However, using such columns induces high back pressure. These low values facilitate the collection of microdialysis samples in the range of microliter, enabling real-time monitoring of neurotransmitter concentrations.

In electrochemical detection processes, the use of salts becomes crucial to increase conductivity and consequently achieve optimal performance. Typically, the aqueous phase of the mobile phase incorporates essential components, such as chelating compounds (e.g., sodium citrate, EDTA), which play a role in preventing coagulation ^[38], an anionic surfactant (sodium dodecyl sulfate, octane sulfonic acid) to prevent interference with lipids and enhance the retention of anionic compounds ^[39], and finally, a buffer (phosphate, citrate).

Most of the time, the pH of the mobile phase is buffered in an acidic environment. The more acidic the eluent, the faster the compounds will elute. Additionally, some compounds are sensitive and degrade more rapidly at basic pH. For instance, this is the case with DA, which oxidizes at a significant rate under basic pH conditions: the half-life at pH 5.6, 7.1, and 7.4 is 13.5 days, 19.7 min, and 4.95 min, respectively ^[40].

Moreover, the mobile phase, predominantly consisting of the aqueous phase with salts, is often augmented with methanol and/or acetonitrile. This strategic addition enhances the eluent's apolar characteristics, ensuring a comprehensive and effective electrochemical detection setup.

Table 2. Recent values of separation, detection and quantification of compounds involved in serotonergic system and their application (non-exhaustive list). All values provided have been standardized to the same unit (mol L^{-1}) for the purpose of comparability.

Reference		HPLC	-ECD Condition	S	Applic	ation
Reinhoud et al. (2013) ^[10]	Methods and Application	C ₁₈ column (1.0 × Flow Column Inject Mobile phase: 100 citric acid, 8 mM k ACI Detection: GC w	100 mm, 1.7 μ m parate = 50 μ L min ⁻¹ temperature = 37 ° tion volume = 5 μ L 0 mM phosphoric ac (CI, 0.1 mM EDTA = OSA. N/H ₂ O (8/92; <i>v</i> / <i>v</i>) pH = 3 vorking electrode (+ Ag/AgCl)	articles size) ² C cid, 100 mM and 2.8 mM 0.65 V vs.	Development method determin monoa concentra applicati microdial prefronta	of analytical for the lation of mines tions and ion to a ysis in a l cortex.
	Detection (mol L ⁻¹)	5-HT	5-HIAA	DA	DOPAC	HVA
	(11012)					

Reference		HPLC-ECD Conditions Application					tion
		LOD	8.3 × 10 ⁻¹¹	3.5×10^{-11}	4.2 × 10 ⁻¹¹	5.0×10^{-11}	4.7 × 10 ⁻¹¹
Ferry et al. (2014) ^[41]	Methods and Application	C ₁₈ colu Mobile p p Detec	mn (0.32 = Flow Columr Injec hase: 140 KCl, 0.1 MeC H = 5 (adj ction: GC v	× 100 mm, 1.9 μ m partie rate = 8.5 μ L min ⁻¹ temperature = 40 °C tion volume = 1 μ L mM potassium phosphe mM EDTA, 6 mM OSA. DH/H ₂ O (6/94; <i>v</i> / <i>v</i>) usted with 10 mM NaO vorking electrode (+0.45 Ag/AgCl)	cles size) ate, 8 mM H) 5 V vs.	Development o method fo determina monoam concentratio applicatio microdialysis in hippocan	f analytical or the tion of ines ons and on to o the dorsal npus
				5-HT	DA	3-M1	Г
	Detection (mol L ⁻¹)	LOD	:	1.5×10^{-9}	7.5 × 10 ⁻¹⁰	1.5 × 1	0 ⁻⁹
		LOQ	Į	5.0×10^{-9}	2.5 × 10 ⁻⁹	5.0 × 1	0 ⁻⁹
Schou- Pedersen	Methods and Application	C ₁₈ colu Injecti potassiu pH Deteo	umn (4.6 × Flow Columr on volume um dihydro MeC I = 3.12 (au ction: Poro ('	a 100 mm, 2.6 μm partic rate = 0.8 mL min ⁻¹ temperature = 30 °C e = 20 μLMobile phase: ogen phosphate, 2 mM c mM EDTA. vH/H ₂ O (10/90; <i>v/v</i>) djusted with 1 M citric a us graphite working ele +0.40 V vs. Pd)	cles size) 70 mM OSA, 0.1 ccid) ectrode	Developm chromatograph for the quantit monoamine I sub-regions of brain (intrace extracellu	ent of hic method fication of NTs from guinea pig Ilular and Jlar).
(2016) ^[<u>42</u>]			5-HT	5-HIAA	DOPAC	DA	HVA
	Detection	LOQ	8.8 × 10 ⁻⁹	3.8×10^{-9}	3.6 × 10 ⁻⁹	1.0×10^{-8}	1.2×10^{-8}
	(mol L ⁻¹)	L.R.	$8.8 \times 10^{-9} - 1.0 \times 10^{-6}$	3.8 × 10 ⁻⁹ -1.0 × 10 ⁻⁶	3.6×10^{-9} -1.0 × 10 ⁻⁶	1.0 × 10 ⁻⁸ – 7.5 × 10 ⁻⁷	1.2 × 10 ⁻⁸ –5.0 × 10 ⁻⁷
Van Dam et al. (2014) ^[43]	Methods and Application	C ₁₈ colu Colu Mobile µ 50 mM ci	umn (1.0 × Flow Imn tempe Inject phase: 8 m tric acid, 0	250 mm, 3.0 μm partic rate = 40 μL min ⁻¹ erature = from 30 °C to 3 tion volume = 50 μL nM KCl, 50 mM phosph 0.1 mM EDTA, from 1.8 OSA.	cles size) 36 °C oric acid, to 2.2 mM	Development o method fo quantification o amines and m in human bra	f analytical or the of biogenic etabolites in tissue.

Reference			HPLC-	ECD Conditions		Applic	ation	
		N pH Detecti	/leOH/H ₂ O (= from 3.0 t on: GC wor +0.6	(from 13/87 to 17/83; o 3.6 (adjusted with N king electrode (from - 7 V vs. Ag/AgCl)	<i>v/v</i>) NaOH) +0.63 V to			
			5-HT	5-HIAA	DOPAC	DA	HVA	
	Detection (mol L ⁻¹)	L.R.	5.3 × 10 ⁻¹⁰ - 1.8 × 10 ⁻⁷	2.2×10^{-10} -7.7 × 10^{-8}	2.8 × 10 ⁻¹⁰ -1.6 × 10 ⁻⁷	2.7 × 10 ⁻¹⁰ –1.8 × 10 ⁻⁷	5.8 × 10 ⁻¹⁰ -3.2 × 10 ⁻⁷	
Pantiya et al. (2024) [44]	 Methods and Application C₁₈ column (3.0 × 500 mm, 2.6 µm particles size) Flow rate = 0.5 mL min⁻¹ Column temperature = 25 °C Injection volume = 25 µLMobile phase: 130 mM sodium phosphate monobasic, 20 mM orthophosphoric acid, 2 mM sodium dodecyl sulfate, 50 µM EDTA. ACN, MeOH, H₂O (5/10/95; v/v/v) pH = 3.2 (adjusted with phosphate buffer) Detection: GC working electrode (+0.50 V vs. Ag/AgCl) 				icles size) 130 mM mM ecyl sulfate, 95; <i>v/v/v</i>) puffer) 50 V vs.	Development method quantification metabolites ir microdial	ent of analytical od for the ion of NTs and s in brain mice dialysates.	
			5-HT	5-HIAA	DA	HV	A	
	Detection (mol L ⁻¹)	LOD	3.1 × 10 ⁻¹⁰	5.4×10^{-10}	3.7 × 10 ⁻¹⁰	4.1 × 1	10 ⁻¹⁰	
		LOQ	3.9 × 10 ⁻¹⁰	5.8×10^{-10}	4.2 × 10 ⁻¹⁰	4.3 × 1	.0 ⁻¹⁰	
Allen et al. (2017) ^[<u>45</u>]	Methods and Application	C ₁₈ col Injecti sodium pH Detec	umn (3.2 × Flow r Columr on volume = acetate, 20 octyl sult ACN = 3.3 (adjus tion: Dual w	150 mm, 3.0 μ m part ate = 0.6 mL min ⁻¹ n temperature = N/A = 40 μ LMobile phase: mM citric acid, 0.38 m fate, 0.15 mM EDTA. J/H ₂ O (5/95; <i>v/v</i>) sted with glacial acetio orking electrode (-0. +0.375 V)	icles size) 100 mM mM sodium c acid) 22 V and	Development method quantifica monoamin metabolites tissue of	of analytical for the ation of nes and s in brain f mice.	
	Detection		5-HT	5-HIAA	DOPAC	DA	HVA	
	(LOD	1.7 × 10 ⁻⁹	6.5×10^{-10}	7.4 × 10 ⁻¹⁰	8.2 × 10 ⁻¹⁰	4.1 × 10 ⁻¹⁰	
			LOQ	3.6 × 10 ⁻⁹	1.3 × 10 ⁻⁹	1.5 × 10 ⁻⁹	1.6 × 10 ⁻⁹	1.4×10^{-9}

Reference			HPLC	-ECD Condition	าร	Applic	ation
		L.R.	3.6 × 10 ⁻⁹ - 1.7 × 10 ⁻⁴	1.3 × 10 ⁻⁹ -7.9 × 10 ⁻⁵	1.5 × 10 ⁻⁹ –8.9 × 10 ⁻⁵	$1.6 \times 10^{-9} -$ 2.0×10^{-4}	1.4 × 10 ⁻⁹ –8.2 × 10 ⁻⁵
Yardimci et al. (2023) [46]	Methods and Application	C ₁₈ colo Mobile citrate, (Glacia P Detec	umn (4.6 × Flow Columr Inject phase: 35 0.16 mM E al acetic ac (0.11/0 0H = 4.9 (a ction: GC v	 250 mm, 5.0 μm p rate = 1 mL min⁻¹ temperature = 36 tion volume = 20 μl mM citric acid, 19 DTA, 1.1 mM hepta cid/tetrahydrofuran/ .3/2.5/97.085; v/v/u udjusted with 10 M working electrode (Ag/AgCl) 	oarticles size) °C MM sodium asulfonic acid. /MeOH/H ₂ O //v) NaOH) +0.50 V vs.	Analysis in hy and subcort	vpothalamic ical nuclei
	Detection		5-HT	5-HIAA	DA	DOP	AC
	$(\text{mol } L^{-1})$	LOQ	5.7 × 10 ⁻⁷	5.2×10^{-7}	6.5 × 10 ⁻⁷	6.0 × 1	10 ⁻⁷
Du et al. (2018) ^[47]	Methods and Application	C ₁₈ coli Mobile pH Detec	umn (4.6 × Flow Columr Inject e phase: 2 AC I = 4.5 (ad tion: BDD	 250 mm, 5.0 μm p rate = 1 mL min⁻¹ temperature = 25 tion volume = 20 μl 5 mM sodium citra EDTA. EN/H₂O (5/95; v/v) justed with 1 M ace working electrode Ag/AgCl) 	oarticles size) °C L te, 0.01 mM etic acid) (+0.70 V vs.	Analytical develop	method oment
				5-HT		5-HI.	AA
	Detection	LOD		2.1×10^{-8}		1.6 × 1	10 ⁻⁸
	(mol L^{-1})	LOQ		2.8×10^{-8}		4.2 × 1	10 ⁻⁸
		L.R.		$2.8 \times 10^{-8} - 1.1 \times 10^{-8}$.0 ⁻⁶	2.6×10^{-8} -2	2.6×10^{-6}
Zhang et al. (2016) [48]	Methods and Application	C ₁₈ coli Mobile p⊢	umn (4.6 × Flow Columr Inject e phase: 2 AC I = 4.5 (ad	 250 mm, 5.0 μm p rate = 1 mL min⁻¹ temperature = 25 tion volume = 20 μl 5 mM sodium citra EDTA. :N/H₂O (5/95; v/v) justed with 1 M ace 	oarticles size) °C L te, 0.01 mM etic acid)	Determinat concentra monoamines cortex and hi tissu	ion of the tions of NTs in rat opocampus es.

Reference			HPL	C-ECD Co	nditions		Applic	cation		
	Detection: BDD working electrode (+0.70 V vs. Ag/AgCl)									
			5-HT	5-HIAA	DA	DOPAC	3-MT	HVA		
		LOD	2.3 × 10 ⁻⁸	1.1 × 10 ⁻⁸	2.6 × 10 ⁻⁸	1.2 × 10 ⁻⁸	3.6 × 10 ⁻⁸	2.7 × 10 ⁻⁸		
	Detection (mol L ⁻¹)	LOQ	8.5 × 10 ⁻⁸	3.1 × 10 ⁻⁸	9.8 × 10 ⁻⁸	4.8 × 10 ⁻⁸	1.2×10^{-7}	8.2 × 10 ⁻⁸		
		L.R.	8.5 × 10 ⁻⁸ – 1.4 × 10 ⁻⁶	3.1 × 10 ⁻⁸ – 7.9 × 10 ⁻⁷	9.8 × 10 ⁻⁸ – 2.3 × 10 ⁻⁶	6.0 × 10 ⁻⁸ –3.0 × 10 ⁻⁶	$1.2 \times 10^{-7} -$ 1.8×10^{-6}	8.2 × 10 ⁻⁸ -1.4 × 10 ⁻⁶		
Jiang et al. (2015) ^[49]	Methods and Application	C ₁₈ co Mob ph Dete	lumn (4.6 Flov Colum Injec bile phase: nosphate, (Me ection: GC	× 250 mm, 5 w rate = 1 m n temperatu ction volume 50 mM pota 0.1 mM octa OH/H ₂ O (5/4 pH = N/4 working elec Ag/AgCl	5.0 μ m par $L min^{-1}$ re = 30 °C $re = 10 \muLassium dihire sulfonio 95; v/v)Actrode (+0.1)$	ticles size) ydrogen c acid. .70 V vs.	Developm analytical r monoamir human	ent of the nethod for nes NTs in urine.		
	Detection				5-HT		D	A		
	(mol L^{-1})	LC	DD		6.1 × 10 ⁻	-8	3.9 ×	10 ⁻⁸		
Lokhande et al. (2022) ^[50]	Methods and Application	$\begin{array}{l} C_{18} \mbox{ column } (4.6 \times 250 \mbox{ mm}, 5.0 \mbox{ \mum particles size}) \\ \mbox{ Flow rate = } 1.3 \mbox{ mL min}^{-1} \\ \mbox{ Column temperature = } 35 \ ^{\circ}\mbox{C} \\ \mbox{ Injection volume = } 20 \mbox{ \muL} \\ \mbox{ Mobile phase: } 50 \mbox{ mM potassium dihydrogen} \\ \mbox{ phosphate, } 0.99 \mbox{ mM SOS and } 53 \mbox{ \muM EDTA}. \\ \mbox{ MeOH/H}_2\mbox{O} \ (12/88; \mbox{ v/v}) \\ \mbox{ pH = } 2.5 \ (adjusted \mbox{ with } 85\% \mbox{ phosphoric acid}) \\ \mbox{ Detection: BDD \mbox{ working electrode (+0.70 \mbox{ vs.} \\ \mbox{ Ag/AgCl}) \\ \end{array}$								
					5-HIAA		HV	/A		
	Detection (mol L^{-1})	LC	QC		6.5 × 10 ⁻	-8	6.9 ×	10 ⁻⁸		
		L.	.R.	6.5 >	< 10 ⁻⁸ –2.6	× 10 ⁻⁶	6.9×10^{-8} -	-2.7 × 10 ⁻⁶		

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Abreviations: N/A: not available, LOD: limit of detection, LOQ: limit of quantification, L.R.: linear range, EDTA: ethylendiaminetetraacetic acid, OSA: octane sulfonic acid, SOS: sodium octane sulfonate, ACN: acetonitrile,

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