Diagnosis of Pediatric Obstructive Sleep Apnea

Subjects: Otorhinolaryngology Contributor: Taylor B. Teplitzky, Audrey J. Zauher, Amal Isaiah

Diagnosis of obstructive sleep apnea (OSA) in children with sleep-disordered breathing (SDB) requires hospital-based, overnight level I polysomnography (PSG). Obtaining a level I PSG can be challenging for children and their caregivers due to the costs, barriers to access, and associated discomfort. Less burdensome methods that approximate pediatric PSG data are needed.

Keywords: obstructive sleep apnea ; sleep disordered breathing ; polysomnography

1. Introduction

Sleep-disordered breathing (SDB) is defined as the disruption of normal respiration and ventilation cycles during sleep $^{[1]}$. In children, these disruptions can range from mild snoring to obstructive sleep apnea (OSA). Pediatric OSA affects an estimated 1.2–5.7% of non-obese children $^{[2][3][4]}$ and almost 60% of obese children $^{[5]}$ in the United States. Like childhood obesity $^{[6]}$, the prevalence of pediatric OSA is expected to rise. Besides obesity $^{[2]}$, other risk factors for pediatric OSA include adenotonsillar hypertrophy $^{[8]}$, craniofacial anomalies $^{[9]}$, and neuromuscular disorders $^{[10][11]}$.

In children, OSA can negatively impact quality of life if left untreated ^[12]. Pediatric OSA has been associated with impaired growth and development ^[13], as well as behavioral and neurocognitive dysfunction ^[14]. The first-line treatment is adenotonsillectomy (AT), which results in the improvement or resolution of symptoms in most children ^{[10][15][16]}.

Level I polysomnography (PSG) is an overnight evaluation performed in an accredited sleep laboratory. The session is attended by a sleep technician and includes a minimum of seven parameters: electrooculography (EOG), electroencephalography (EEG), chin electromyography (EMG), airflow, respiratory effort, oxygen saturation, and electrocardiography (ECG) ^[17]. The severity of OSA is determined by the apnea-hypopnea index (AHI), or the frequency of partial or complete reduction in airflow. Mild, moderate, or severe OSA correspond to AHI thresholds of less than 5, 5–9, and 10 and over, respectively. Pediatric OSA is diagnosed when the PSG reports an AHI ≥ 1 ^[17].

Level I PSG is currently the only approved method to diagnose pediatric OSA ^{[10][18]}. The American Academy of Sleep Medicine (AASM) ^[19] and the American Academy of Pediatrics (AAP) ^[10] recommend PSG to screen children with any SDB symptoms. The American Academy of Otolaryngology–Head and Neck Surgery (AAO–HNS) recommends PSG prior to AT in children under 2 years of age or in those with obesity, craniofacial or neuromuscular disorders, Down syndrome, sickle cell disease, or mucopolysaccharidoses ^[16]. The AAO–HNS also recommends PSG if the need for surgery is uncertain or if the severity of the SDB cannot be explained by a physical exam ^[16].

While a PSG is routinely recommended preoperatively by the AASM and the AAP, only 10% of children who are scheduled for AT undergo a PSG ^[20]. This is likely due to the significant barriers to obtaining a PSG. For example, there is limited access to certified sleep laboratories and providers with the technical expertise necessary to diagnose OSA in infants and young children ^[21]. The PSG itself is burdensome, requiring the use of multiple monitors during sleep in an unfamiliar laboratory environment ^[21]. As caregivers need to be present throughout the duration of the test, their employment, productivity, and responsibilities to other members of the family may be impacted. Finally, the cost of PSG in the United States ranges from USD 1000 to USD 4000, posing a marked strain on the healthcare system ^{[22][23]}.

2. Alternative Approaches to Polysomnography—Objective Measures

2.1. Single Channel Recordings

Of the nine parameters included in a level I PSG ^{[21][23][24]}, cardiovascular, pulse oximetry, body position, and respiratory events have each been examined as potential single-channel equivalents to a standard PSG.

2.1.1. Cardiovascular

Full electrocardiogram (ECG) recordings from overnight PSG have a sensitivity of 85% and specificity of 81% to detect OSA in children (ages 1.2–16 years) when using the modified quadratic discriminant analysis classification system described by Shouldice et al. ^[25]. Due to the impact of intermittent hypoxia on the heart, ECG-measured heart rate variability may stratify chronic upper airway obstruction ^{[23][26][27][28]}. Predictable changes in heart rate variability are noted when evaluating children (ages 3–8 years) with confirmed OSA by PSG ^{[28][29]}. Though not accepted by itself, the utility of integrating cardiac rhythm analysis and ECG findings with other screening metrics has not been studied.

2.1.2. Pulse Oximetry

The utility of pulse oximetry as a single-channel recording for predicting pediatric OSA has been extensively studied. Brouillette et al. ^[30] concluded that pulse oximetry can be used for the potential diagnosis of OSA in infants (ages less than 1 year) with SDB and adenotonsillar hypertrophy. The authors found that a positive nocturnal oximetry trend had a 97% positive predictive value for OSA in infants suspected of having OSA ^[30]. Models created by Garde et al. ^[31] demonstrated acceptable accuracy, sensitivity, and specificity when using pulse oximetry to screen for OSA at AHI cut-offs of 1, 5, and 10. The authors concluded that pulse oximetry-based screening for OSA at different AHI thresholds may determine referral thresholds for level I PSG ^[31]. A meta-analysis performed by Wu et al. ^[32] found that pulse oximetry had the highest overall specificity when compared to the Pediatric Sleep Questionnaire (PSQ) and the OSA-18 Quality of Life Survey (OSA-18). When combined with the PSQ, the authors noted that pulse oximetry can detect OSA in children (ages 2.9–16.7 years) in instances when formal PSG is unavailable ^[32].

The McGill Oximetry Score (MOS) developed by Nixon et al. ^[33] could predict OSA severity, enabling clinicians to prioritize treatment for those with more severe SDB. The MOS is based on the number of clusters of desaturation events and the number of times arterial oxygen percent saturation drops below 90%, 85%, and 80% ^[33]. The scores, which range from 1 to 4, indicate a normal/inconclusive OSA study (MOS = 1), mild OSA (MOS = 2), moderate OSA (MOS = 3), or severe OSA (MOS = 4) ^[33]. In an evaluation of a MOS-based treatment algorithm, Horwood et al. ^[34] concluded that the MOS stratifies SDB in resource-limited scenarios.

The ability of the MOS to detect pediatric OSA and serve as a diagnostic alternative to PSG has been challenged. A study of healthy children (ages 4–18 years) concluded that pulse oximetry was insufficient to detect OSA ^[35]. Additionally, in a study of children (ages 3–15 years) with adenotonsillar hypertrophy, a high rate of OSA was detected in those assigned a MOS of 1 (inconclusive) ^[36]. However, the diagnostic accuracy of the MOS may improve with serial overnight oximetry readings. Specifically, two nights of pulse oximetry readings can generate a MOS that supports a diagnosis of OSA when the MOS is at least 2.68 ^[37].

Outside of the MOS system, abnormal pulse oximetry readings alone may have utility for risk stratification. Pavone et al. ^[38] found that when PSG is not available, abnormal pulse oximetry readings can predict the child's need for AT. Similarly, Saito et al. ^[39] concluded that pulse oximetry can determine indications for AT. Hoppenbrouwer et al. ^[40] examined pulse oximetry variability in children (mean age 8.3 years) over two consecutive nights: one night of hospital-based PSG followed by one night of home oximetry. The authors found no significant variability between the oximetry measurements obtained in the hospital versus the home setting ^[40].

2.1.3. Body Position

Body position is measured during formal PSG using an actigraph. While a wrist-worn device is most often used ^[21], sensors worn on the hip or pressure sensors placed in the bed are alternatives ^[22]. In addition to body position, the actigraph also determines total sleep time (TST), wake after sleep onset (WASO), and sleep efficiency ^[21]. Multiple actigraph models are available, from the sleep-focused Actiwatch-2[®] (Phillips Respironics, Amsterdam, The Netherlands) and the Motionlogger[®] Sleep Watch (Ambulatory Monitoring, Ardsley, NY, USA) to the commercially-available Fitbit Ultra[®] (Fitbit, San Francisco, CA, USA) and UP[®] (Jawbone, San Francisco, CA, USA) ^[21].

In children (ages 5–12 years) with suspected OSA, the Actiwatch-2 demonstrated a sensitivity of 88% (i.e., ability to detect sleep) and a specificity of 46% (i.e., ability to detect wake) ^[41]. The Actiwatch-2 also underestimated TST and sleep efficiency ^[41]. Studies of other actigraphs in school-age and adolescent children (ages 3–18 years) found similar patterns of poor specificity but accurate and sensitive estimates of TST, WASO, and sleep efficiency ^{[42][43]}.

Actigraphy may have greater diagnostic utility when combined with oximetry data. Using machine learning to generate comparison models, Bertoni et al. ^[44] found that, when combined with the oxygen desaturation index, actigraphy can predict severe OSA in children (ages 2–17 years).

2.1.4. Respiratory Events

During formal PSG, respiratory events are captured by an oronasal thermal airflow sensor or a nasal pressure transducer $\frac{[21]}{2}$. These systems are primarily used in laboratory and research settings. The results of this technology in children are mixed. An observational study of 47 children aged 2–14 years found that the nasal pressure transducer detected more apneas and hypopneas than the thermal airflow sensor $\frac{[45]}{2}$. A study of 14 infants (ages 0.5–9.4 months) with suspected OSA noted a nasal pressure transducer was more accurate than a thermal airflow sensor at detecting hypopneas versus apneas $\frac{[46]}{2}$. In contrast, a more recent study of 172 children under 3 years old concluded that the nasal pressure transducer had limited ability to detect obstructive events $\frac{[47]}{2}$.

2.2. Home Sleep Apnea Testing

Home sleep apnea testing (HSAT) is an unattended, home-based sleep study that utilizes portable and wearable monitors with the goal of replicating level I PSG ^[23]. Pediatric HSAT uses fewer resources and is more cost efficient than level I PSG, with the additional benefits of increased patient comfort and improved accessibility ^{[18][21]}. The AASM does not currently support the use of HSAT to diagnose pediatric OSA. Difficulties in feasibility, validity, identifying arousals and hypoventilation, issues with use in young children or children with comorbidities, and differences in body sizes are the cited challenges ^[18].

However, the feasibility of HSAT in children (under 16 years of age) has been demonstrated in multiple studies ^{[48][49][50]}. A recent systematic review and meta-analysis demonstrated that HSAT had a pooled sensitivity of 74% and a pooled specificity of 90% for detecting OSA in children (ages 1–18 years) ^[51]. In children aged 2–17 years, HSAT and PSG yielded similar AHI and the lowest oxygen saturation measurements in children \geq 6 years old ^[52]. Similarly, in a study of children aged 5–18 years, HSAT demonstrated excellent concordance with level I PSG ^[53]. The authors concluded that HSAT is a feasible and comparable alternative to level I PSG ^[53]. A Spanish study found that home respiratory polygraphy is a potential reliable alternative to in-laboratory PSG in children aged 2–14 years ^[54]. Despite these data, HSAT remains unapproved in children.

While the ability of HSAT to diagnose pediatric OSA holds promise, its current use is limited to a screening method, a role in which it has been successful ^[51]. To limit the unnecessary use of PSG, home testing may serve as an initial assessment before formal testing is considered ^[55].

2.3. Sound Analysis

During a standard PSG, the brain is monitored for progression through sleep stages. Adult literature has demonstrated changes in breathing patterns associated with different sleep stages [56][57][58][59][60][61], prompting the evaluation of sleep sounds in children. Rembold et al. [62] described the pathophysiology of high-frequency inspiratory sounds (HFIS) generated by children (ages 6-12 years) with obstructive sleep-disordered breathing. Children produce such sounds from a narrowed upper airway, which subsequently acts as a resonating chamber. Similarly, HFIS were shown to be a marker of disturbed breathing in children (ages 6–12 years) with adenotonsillar hypertrophy [63]. With this knowledge, the study of sleep sounds in children as a component of OSA diagnosis or screening has been tested. Using tracheal sounds combined with suprasternal pressure to score respiratory events in children (ages 1-16 years), the sensitivity of detecting an apnea was 86%, and hypopnea was 77% [64]. Similarly, the authors noted a 95% sensitivity and 100% specificity for the detection of an obstructive apnea, a 95% sensitivity and 97% specificity for a mixed apnea, and a 91% sensitivity and 97% specificity for a central apnea [64]. The authors concluded that tracheal sounds with suprasternal pressures have the ability to both detect and characterize apneas and hypopneas in children [64]. The Sonomat system (Sonomedical Pty Ltd., Balmain, NSW, Australia) is a non-invasive mattress pad that can be used in the home without requiring any sensors or monitors to be physically attached to the patient [65]. In a prospective and randomized trial, Sonomat was shown to be reliable and accurate in the diagnosis of adult OSA [65]. The Sonomat was then compared to PSG in children (ages 2-17 years) and found to accurately diagnose OSA [66]. A recent study used the Sonomat to assess snoring and stertor in children (ages 0.8-17.7 years) with OSA and found episodes of these airway sounds occurred more frequently than obstructive events and were associated with sleep disruption [67]. The Sonomat was further found to detect complete and partial airway obstruction in children (under 18 years of age) after sleep surgery [68]. The authors noted the persistence of sleep disturbance, via snoring and stertor, despite improvement in the mixed and obstructive apnea-hypopnea index (MAOHI) [68]. The relationship between snoring sound energy (SSE) and OSA severity, as well as changes in SSE after adenotonsillectomy, were studied in children (ages 6-12 years) [69]. In this article, an SSE of 801-1000 Hertz (Hz) was shown to be significantly related to severe OSA and decreased post-operatively. Similarly, the authors noted that a baseline SSE of 801–1000 Hz significantly predicted surgical success [69]. The authors concluded a potential use of SSE in screening OSA as well as predicting outcomes after OSA treatment ^[69]. Brietzke et al. ^[70] found utility with acoustical analysis of snoring in children (ages 2-15 years), noting that an increasing snoring index and loudness were associated

with increased OSA severity. The authors noted that increased snoring was associated with oxygen desaturations in cases without OSA ^[70].

However, the data on sleep sounds have been mixed. A multivariate analysis comparing clinical variables, home snoring sound analysis, and home sleep pulse oximetry did not identify snoring sound energy as a predictor for severe OSA in children aged 5–12 years $^{[71]}$. A meta-analysis on the acoustic analysis of snoring found that, though accurate, it is not a strong method for diagnosing OSA in those less than 18 years of age $^{[72]}$. Further studies are needed to understand the utility of sleep sounds in pediatric OSA.

2.4. Genetics

OSA is known to cluster in families [73][74], and the study of a genetic component in pediatric OSA confirms it is a heritable trait [75]. However, the genetic inheritance of OSA is likely multifactorial [76], making the identification of causative genes more challenging.

Larkin et al. [77] studied single nucleotide polymorphisms and their association with AHI, noting different gene associations in different populations. The authors found a potential role for genes operating through concomitant diseases, such as obesity, that influence OSA phenotypes [72]. An association between craniofacial anomalies and OSA has been described [78], leading to the study of genes related to structural development. In a study of children with Class III malocclusion, silent mutations in PHOX2b, a gene involved in neural crest cell development for facial and skull growth ^[79], were found in 32% of children with breathing dysfunction but none of the controls [80]. Additionally, studies about the relationship between OSA and obesity have identified several possible genetic interactions. Ye et al. [81] noted increased expression of liver X receptors, which are important in the control of lipid metabolism. Fatty-acid binding protein 4 (FABP4) gene polymorphisms led to increased morning FABP4 levels in children (ages 2-12 years) with obesity and OSA [82]. Interestingly, this protein was elevated in the morning serum in children (ages 2–12 years) with OSA without obesity [82], indicating these SNPs may portend cardiometabolic risk. Apolipoprotein E (APOE) is also involved in lipid metabolism and has been studied in pediatric OSA. The APOE 4 allele was specifically more frequently identified in children (ages 5-7 years) with OSA, with a higher incidence in those who have neurocognitive effects [83]. A genome-wide association study in children (ages 4-9 years) with OSA noted altered expression of gene clusters involved in inflammation in circulating leukocytes, implying adaptive and end-organ injury in the setting of OSA [84]. Epigenetic studies have shown gene modifications related to pediatric OSA [85], broadening the genetic study to include methylation patterns. The literature supports a genetic influence on metabolic pathways as well as the structural anatomy involved in pediatric OSA, though further research is needed to characterize these relationships.

2.5. Imaging

Cephalometry involves standardized views of the lateral head and neck, allowing for visualization of skeletal and soft tissue structures of the upper airway ^[86]. Using cephalometry, Shintani et al. ^[87] confirmed a high prevalence of adenotonsillar hypertrophy in children with OSA. In addition, reduced maxillary and mandibular protrusion and differences in hyoid positioning were significantly associated with OSA ^[87]_[88]. Ozdemir et al. ^[89] used cephalometry as a screening tool and found a significant correlation between these data and AHI in children (ages 4–12 years) with OSA. A systematic review and meta-analysis of craniofacial and upper airway morphology identified a significant association between craniofacial disharmony on cephalometric studies and pediatric sleep-disordered breathing in children less than 18 years of age ^[90]. However, the authors did not support a causal relationship between facial structure and sleep-disordered breathing ^[90]. When compared to magnetic resonance imaging (MRI), cephalometric analysis was found to be a valid method to measure nasopharyngeal and retropalatal dimensions in children aged 4.8–9.8 years ^[91]. Limitations to cephalometry include that the images are obtained upright in awake patients, though OSA affects children in the supine position while asleep, potentially reducing their diagnostic properties ^[86]. Similarly, the quality of these images is predicated on their positioning, which can alter the results. The images are also limited to 2 dimensions, causing a theoretical loss of important information.

Lateral neck X-rays are plain X-rays of the neck that can provide data on upper airway dimensions. Brooks et al. ^[92] used lateral X-rays to measure the adenoidal-nasopharyngeal (AN) ratio and found a significant relationship between the AN ratio and the duration of apneas in children aged 0.4–11.6 years. Identification of adenoid hypertrophy on lateral neck X-ray is correlated with the degree of OSA in children aged 4–12 years ^[93]. Xu et al. ^[94] utilized lateral neck X-rays as part of a clinical evaluation in children aged 4–18 years and found that upper airway narrowing via adenoid hypertrophy was a significant predictor of OSA. The utility of lateral neck X-ray for identifying or confirming tonsillar hypertrophy is limited in children (mean age 6.2 years) ^[95] and therefore should be reserved for assessment of the adenoid pad.

MRI allows for cross-sectional evaluation of the upper airway and offers the option of 3D reconstruction as well as the possibility of dynamic images with cinematic (cine) MRI [86]. A benefit of MRI over computerized tomography (CT) is the lack of radiation. However, these tests are long and require the patient to be still, a common challenge in young children. To obtain a useful MRI, sedation may be required, which has inherent risks but may also alter the upper airway dimensions relative to natural sleep [86]. In a study of children aged 7-12 years with PSG-diagnosed OSA, MRI found a positive correlation between tonsil size and the size of the soft palate, with an inverse relationship between AHI and the volume of the oropharynx [96]. The smallest region of the upper airway was found to be the retropalatal airway, which was smaller in those with more severe OSA [96]. MRI tests in 40 children (ages 4–14 years) with diagnosed OSA by PSG were retrospectively evaluated for 25 measurements [97]. The authors identified significant differences in both soft tissue and bony anatomy between those with and without OSA. Specifically, soft tissue differences included a smaller upper airway volume, nasopharyngeal airway, oropharyngeal airway, larger soft palate, and larger tonsils and adenoids in those with OSA [97]. Skeletal differences included a lower hyoid position, smaller sella-nasion-supramentale angle, and smaller mandibular volume in children with OSA [97]. Cine MRI is a specialized MRI study first described by Donnelly et al. [98]. It is a dynamic test, affording the benefit of simultaneous assessment of the entire airway during sleep to identify the site of persistent obstructive airway motion [99][100]. Cine MRI does require anesthesia, and protocols have been made to approximate natural sleep [99], as well as the imaging sequences to obtain an adequate test [100]. Due to the constraints of cost, time, and the need for anesthesia, cine MRI is classically reserved for children with persistent OSA after adenotonsillectomy.

CT scans are fast, noninvasive, and typically readily available. Their main drawback is radiation exposure, though protocols have evolved to reduce the dose in children ^[86]. Three-dimensional models derived from CT scans in children (ages 3–16 years) were found to predict OSA severity better than clinical scores of upper airway patency ^[101]. A recent study comparing children under 10 years old with or without OSA found morphological data on the imaging, combined with clinical indices such as habitual snoring, mouth breathing, and adenoid faces, had high diagnostic value for OSA ^[102]. Further studies are needed to assess the role of CT in pediatric OSA diagnosis.

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