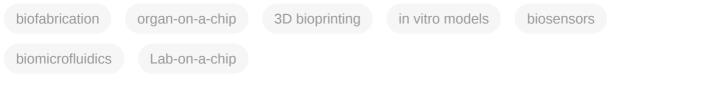
3D Printing in Organ-on-a-Chip Platforms

Subjects: Engineering, Biomedical

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Three-dimensional (3D) in vitro models, such as organ-on-a-chip platforms, are an emerging and effective technology that allows the replication of the function of tissues and organs, bridging the gap amid the conventional models based on planar cell cultures or animals and the complex human system. Hence, they have been increasingly used for biomedical research, such as drug discovery and personalized healthcare. A promising strategy for their fabrication is 3D printing, a layer-by-layer fabrication process that allows the construction of complex 3D structures.



1. Introduction

The aforementioned preclinical models used in biomedical investigation are outlined in <u>Figure 1</u>, highlighting the evolution of cell-culture models from simple two-dimensional to complex OoC platforms with 3D bioprinted models.

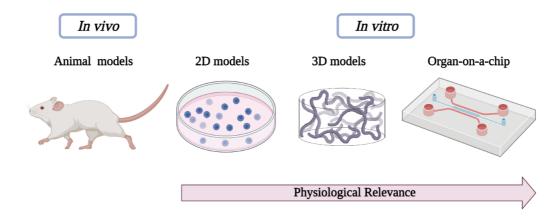


Figure 1. Schematic diagram showing preclinical models used in biomedical research.

2. 3D Printing Techniques and Their Applications to Organon-a-Chip Platforms

2.1. 3D Printing Techniques

3D printing has become a growing field in different areas and it has gained great interest, because of the ability to build complex structures through a layer-by-layer process with different materials in an affordable way ^[18]. For these reasons, some authors have been using 3D printing techniques to rapidly fabricate the microfluidic models and holders for OoC devices (<u>Table 1</u>).

Device	Printing Method	Applicatio	on	Main Observations	Ref.
Vessel-on- a-chip	-	Produce molds with diverse forms of channels.	Developed by dynamic laters with different forms of an incorporate in the artist different forms of an incorporate in the artist different form of an incorporate in the artist different form ref. [19]. Copyright 2018 John Wiley and Sons.	A simple and cytocompatible approach was developed for fabricating hydrogel-based user-defined chips, suitable for the growth of organ or vascularized tissue models.	[<u>19]</u>
Lung cancer-on- a-chip	Inkjet	3D-printed chip holder and elastomeric microfluidic channels and microfluidic connectors for cell culture media routing on the higher part of the glass.	Stematic interoliticitic game dire table future The properties of the stematic The stematic stematic The stematic stematic stematic The stematic stematic stematic The stematic stematic stematic The stematic stematic stematic stematic stematic stematic The stematic stema	This lung cancer-on-chip system, includes integrated biosensors for real-time monitoring of physiological events, can be used with any organ tissue or monolayer micro-tumor models for on-chip toxicity studies.	[<u>20</u>]

Table 1. 3D printing techniques used to fabricate OoC platforms.

Device	Printing Method	Applicatio	on	Main Observations	Ref.
Metastasis- on-a-Chip	Plaster- based 3D printing	3D-printed inverted chamber/channel structures as molds.	Reprinted with permission from ref. ^[21] . Copyright 2016 John Wiley and Sons.	This system supports some aspects of the phenomena of metastasis, allowing to study the translocation of metastatic tumor cells from the primary tissue site to the downstream tissue site.	[<u>21</u>]
Vessel-on- a-chip	Extrusion- based 3D printing	3D printing of channel prototypes with carbopol gel	Composed and the second s	It is presented a highly affordable and practical approach in the manufacture of PDMS devices with closed fluid channels, which have great potential to reconstitute a human endothelium-on-a- chip	[2]
Kidney-on- a-chip	FDM	3D-printed template for conventional soft lithography fabrication of PDMS-based OoC	Indexa Mondair Automatication and the second and th	It is demonstrated the application of a 3D-printed template and a common cutter machine to provide a simple and affordable fabrication of OoC.	[<u>22</u>]
Multi- Organ-On- a-Chip	Laser SLA with epoxy resin	Produce master models for the chambers and channels of the fluidic device.	Vacular chambers Open chambers Ope	This technology allows the design and rapid mass production of OoC devices.	[<u>23]</u>
Lung-on-a- chip	DLP	3D-printed molds to manufacture a chip model with an open well design and with lower and upper layers to mimic the human lung.	Reprinted from ref. [24].	The fabrication technique allows the chip to be fabricated in less than a day, and the molds can also be utilized for repeated PDMS casting. Therefore, the technique is robust, cost-effective, and simple.	[<u>24]</u>

SLA—stereolithography; FDM—fused deposition modelling; DLP—digital light processing.

The usage of 3D printing techniques to fabricate OoC is simple, cost-effective, robust, and allows the mass manufacture of customized OoC devices. However, attention must be taken in the selection of the 3D printing technique to obtain molds for PDMS casting. For example, molds printed via SLA/DLP methods may not be appropriate for PDMS casting because residual oligomers and monomers on the top of the 3D-printed pieces hamper PDMS polymerization ^[24]. Hence, the development of optimized surface treatments is crucial for ensuring long-term cell viability in OoC devices. Furthermore, the material utilized in 3D printing must be selected taking into account the curing temperature of the casting material in order to prevent material strain and microstructure deformation, which consequently can affect the cell viability.

2.2. 3D Bioprinting Techniques

As previously stated, 3D bioprinting can be described as the spatial distribution in a defined pattern of living cells. The cells are loaded and assembled through layer-by-layer deposition methods assisted by means of a computer, and used for the manufacture of organ analogs and living tissue for a different set of applications, such as pharmacokinetic, tissue engineering, cancer research, and regenerative medicine, among others ^[25]. For this purpose, biocompatible materials, such as alginate, gellan-gum, collagen, fibrin, and gelatin, are usually used to form hydrogels, called bioinks, to encapsulate cells (cf. <u>Table 2</u>) in order to protect them during the printing process.

OoC Platform	Printing Method	Schematic Representation	Cells Types	Bioink	Ref.
Nervous System-on-a- Chip	Micro-extrusion 3D printing strategies	Reprinted with permission from ref. [26]. Copyright 2001 Royal Society of Chemistry.	Schwann cells, superior cervical ganglia and hippocampal neurons and epithelial cells	-	[<u>26</u>]
Central nervous system-on-a- chip	Magnetic bioprinting	• Complete	Spinal cord cells	Neural spheroids	[27]
Multi-tissue OoC with liver, heart and lung organoids	Microextrusion bioprinting	Line Control C	Hepatocyte; stellate; Kupffer iPS; lung fibroblasts, epithelial, and endothelial cells.	Spherical organoids with HA-gelatin hydrogel (liver) and fibrin-gelatin bioink (cardiac).	[<u>28</u>]

Table 2. 3D bioprinting techniques used to fabricate OoC platforms.

OoC Platform	Printing Method	Schematic Representation	Cells Types	Bioink	Ref.
3D vascularized tissue-on-a-chip	Microextrusion bioprinting	e e e e e e e e e e e e e e e e e e e	hMSCs; hNDFs; HUVECs	Vascular ink (pluronic and thrombin) and cell-laden ink (gelatin–fibrin)	[<u>29</u>]
Liver-on-a-chip	Direct write bioprinter		HepG2/C3A cells	Hepatic spheroids and GelMA	[<u>30</u>]
Liver-on-a-chip	Microextrusion bioprinting	Cell type C with hydroget with hydroget hype B hype B hype B hype CL printing for microfluidic channel Printing of channel cover	HepG2; HUVECs.	Gelatin and liver dECM bioinks (collagen type 1)	[1]
Liver-on-a-chip	Microextrusion bioprinting	Blood Flow Bile	HepaRG and HUVECs	Gelatin and liver dECM bioinks (collagen type 1)	[<u>31</u>]
Liver Fibrosis- on-a-Chip	Microextrusion bioprinting	Reprinted with permission from ref. [32]. Copyright 2020 American Chemical Society.	HepaRG, HUVECs and hepatic stellate cells	Gelatin and liver dECM bioinks (collagen type 1)	[32]
Convoluted 3D renal proximal tubules-on-a- chip	Extrusion custom- designed, multi- material 3D bioprinter	Original October Original Original Original Original Office Series Original October Original October Octobe	PTECs-TERT1	Two-part silicone elastomer; Pluronic and thrombin.	[<u>33]</u>
Vessel-like structures-on-a- chip	Coaxial nozzle- assisted extrusion- based bioprinting	Reprinted with permission from ref. [34]. Copyright 2017 American Chemical Society	L929 fibroblasts; endothelial cells and smooth muscle cells	Cell-laden alginate filaments	[<u>34</u>]

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OoC Platform	Printing Method	Schematic Representation	Cells Types	Bioink	Ref.
Vessel-on-a- chip	-	U printing U Bonding → → →	HAECs; HASMC and NIH/3 T3 fibroblast cell lines	GelMA	[<u>35</u>]
Heart-on-a-Chip	Direct write bioprinter with a customized coaxial nozzle	Reprinted with permission from ref. [36]. Copyright 2016 Elsevier	HUVECs	Alginate-GelMA	[<u>36</u>]
Myocardium-on- a-chip	Extrusion-based 3D bioprinting	Reprinted with permission from ref. [37]. Copyright 2020 John Wiley and Sons.	hiPSC-CSs	Non-mulberry silk-based ink GelMA and PEGDMA	[<u>37</u>]
Gut-on-a-chip	Dual cell-printing system supplemented with a core-shell nozzle	Reprinted with permission from ref. [38]. Copyright 2018 American Chemical Society.	Caco-2 cells and HUVECs	Cell-laden collagen bioinks	[<u>38]</u>
Thrombosis-on- a-chip	Embedded extrusion bioprinting	Reprinted with permission from ref. [39]. Copyright 2016 Royal Society of Chemistry.	HUVECs	GelMA	[<u>39]</u>
Tumor array-on- a-chip	On-demand array printing	Axial Motion System	MDA-MB-231 breast tumor cells showed	GelMA	[<u>40</u>]
Placenta-on-a- chip	Extrusion-based 3D bioprinting	Reprinted with permission from ref. [41]. Copyright 2016	Human placental cell line and hMSCs	GelMA	[<u>41</u>]

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1	OoC Platform	Printing Method	Schematic Representation	Cells Types	Bioink	Ref. , Z.; et
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	with integrate	d hinsensors for n	hysiological monitor	ing and toyicity as	sassmant Ri	ochom Eng

with integrated biosensors for physiological monitoring and toxicity assessment. Biochem. Eng. J. iPS_induced pluripotent stem cells; HA—hyaluronic acid; hMSCs—human mesenchymal stem cells; hNDFs— 2020, 155, 107469. human neonatal dermal fibroblasts; HUVECs—human umbilical vein endothelial cells; HepG2—human 21epSkædialaA.caPawarasettypAkcEQEvirihalityS dirktalatiaAedSAkrataSheptadeutitanistanatastasienen derona a 21epSkædialaA.caPawarasettypAkcEQEvirihalityS dirktalatiaAedSAkrataSheptadeutitanistanatastasienen derona a 22e, Habes-primary human aortic endothelial cells; HASMC—human aortic smooth muscle cell line 22. Eho9; S., Fishas-Robiets, A., Niccoliny, A. Ni., Morriss, T.J., Pabhu, C. Y. Hurishtur, tual-model montoring of a sphergids: DFGDMA-polyethylene glycol dimethacrylate: BMECS-induced Programs. Bioeffectron: 2016, 86, 697–705

86, 697–705. It can be seen that 3D printing techniques are versatile and they can be applied to obtain a variety of OoC or multi-23ghantalanh, Buickflagiellous - SPASSEC Hardwell Wisterman CMp; Rowa-&chometaleona-chiptlesselic Gareinp, Ruizoch Buresnarchip, ngthe method arthurd arthur bester as a production of the chip. The Bailes a Polymers 2012, 10, 1238.

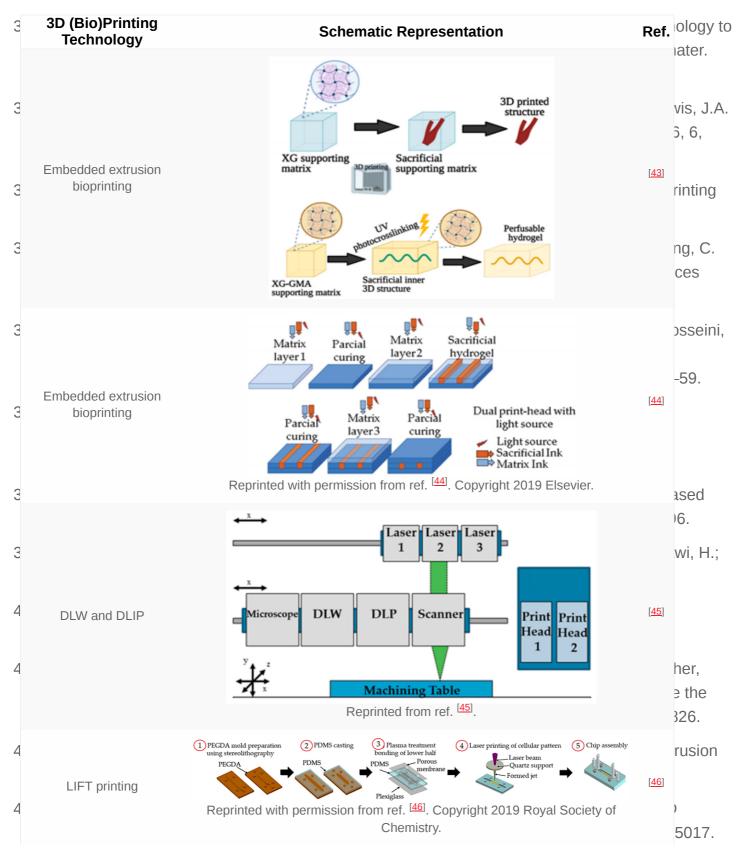
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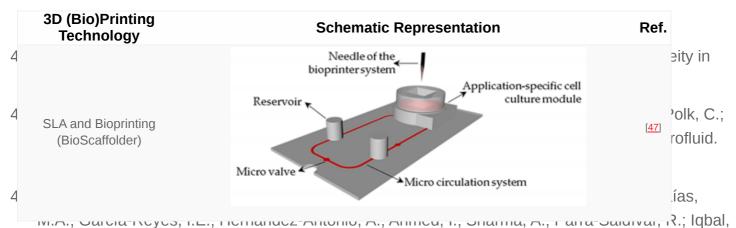
26 Johnsone B.N.: Lancaster K.Z.: Hogue I.B.: Meng, F.: Kong, Y.L.: Enguist I.W.: McAlpine, M.C.: 3D printed nervous system on a chip. Lab Chip 2016, 16, 1393–1400.

2	3D (Bio)Printing Technology	Schematic Representation	Ref.	netic
2	Embedded extrusion bioprinting	Multinozzle printhead	[<u>42</u>]	S.; a-chip of thic
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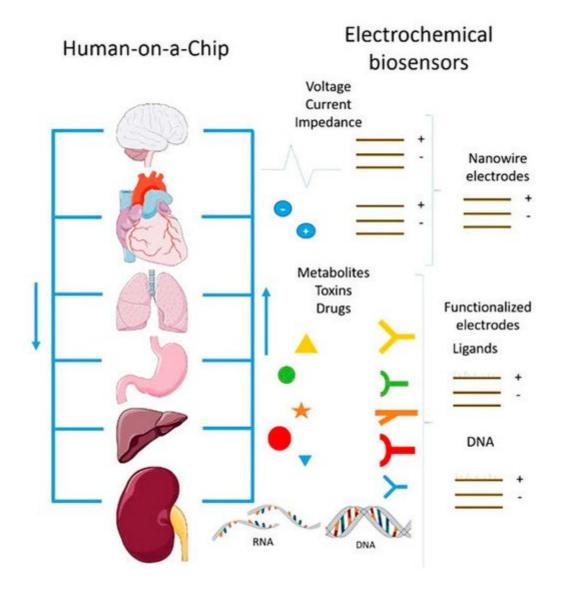
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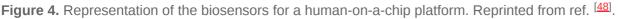


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50 or Matchelld and Lastoratoly.; phatyoeska, old.; place optimizes on a contact united to be incorporated into those platforms to allow for real-time, robust, and autonomous monitoring of the organ models.

In the near future, multi-organ-on-a-chip and, ultimately, human-on-a-chip platforms are expected to be developed. For that purpose, a platform with integrated biosensors will be a huge step towards the advance of OoC platforms, providing physiological metabolism parameters of the organ model, as presented at <u>Figure 4</u> ^[48]. In this way, innovative experimental studies will be possible and as a result it will help to improve our understanding about the evolution of certain pathologies and how they affect the overall system ^[48]. A more comprehensive review on this topic can be found elsewhere ^[49].





4. Future Perspectives

Although great efforts for developing new and feasible 3D (bio)printing techniques have been made, wide-scale adoption and validation are still to be achieved. Through advances in 3D printing technologies, more physiologically relevant OoC models are expected and this will accelerate the commercialization of these models and their practical use in drug discovery to overcome several human diseases. Although the focus of this work lies in 3D (bio)printing, it should be mentioned that the variable "time" has also been integrated, giving rise to 4D bioprinting, where printed items (for example, responsive biocompatible materials or cells) are able to change their functionalities or shapes with time once an external stimulus is imposed ^[50].